



Master's Thesis

# Neural networks for compressing and classifying speakerindependent paralinguistic signals

준언어적 신호 압축 및 분류를 위한 심층 신경망

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# Abstract

Recognizing and classifying paralinguistic signals, with its various applications, is an important problem. In general, this task is considered challenging because the sound information from the signals is difficult to distinguish even by humans. Thus, analyzing signals with machine learning techniques is a reasonable approach to understanding signals. Audio features extracted from paralinguistic signals usually consist of highdimensional vectors such as prosody, energy, cepstrum, and other speech-related information. Therefore, when the size of a training corpus is not sufficiently large, it is extremely difficult to apply machine learning methods to analyze these signals due to their high feature dimensions. This paper addresses these limitations by using neural networks' feature learning abilities. First, we use a neural network-based autoencoder to compress the signal to eliminate redundancy within the signal feature, and we show than the compressed signal features are competitive in distinguishing the signal compared to the original methods such as logistic regression, support vector machine, decision trees, and boosted trees.

**Keyword**: Computational paralinguistics, Neural networks **Student Number**: 2017–22921

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### **Chapter 1. Introduction**

Neural network-based models have achieved state-of-theart performances in diverse applications, such as computer visio n, neural machine translation, recommendation systems, and oth er task-oriented areas [1]-[3]. Along with such impressive ad vancements, statistical speech processing has also demonstrated many advantages when adopting a neural network-based archit ecture. For instance, Amodei et al. [4] demonstrated that a con volutional architecture with a recurrent architecture can achieve great performance in speech recognition due to its abilities to 1 earn more salient features in the time domain and temporal dep endencies within the utterance. Synthesizing speech with a neur al network architecture has also been successful [5] by utilizin g the neural network's feature learning ability to incorporate ea ch text-to-speech module to reduce extensive domain expertis e and complexity.

In addition, diverse areas exist in the area of paralinguistic si gnals, such as analyzing the tone/pitch of the voice, nuance, an d speech with upper respiratory symptoms [6]. Including these, all paralinguistic studies are receiving growing attention providi ng considerable assistance in medical science, psychology, and general engineering fields.

However, one of the biggest difficulties in analyzing paralinguis tic signals lies in its ambiguity that is indistinguishable even by humans. Thus, researchers have adopted various aspects of a signal, such as prosody, energy, and cepstrum, to analyze th e signal. In addition, only a small number of paralinguistic signal s in a dataset is usually acquired in real situations for training t he model, implying that the model is not able to sufficiently lea rn the feature representations. To address this issue, Sahu et al. [7] used adversarial autoencoders for dimension reduction and showed that compressed signal representations do not significa ntly harm overall emotion recognition performance by comparing classification accuracy in original/compressed feature settings.

In this paper, we suggest using various machine learning tec hniques, such as autoencoders (AE), principal component analy sis (PCA), and linear discriminant analysis (LDA), for feature dimension reduction on two different feature sets extending th e research in [7]. With the compressed features, we adopt ma chine learning models such as multilayer perceptron (MLP), su pport vector machine (SVM), logistic regression (LR), decision tree (DT), and boosted tree (XGB) for classifying the paralin guistic signals.

Experimental results show that most of the models trained w ith the compressed features provide competitive classification a ccuracy compared to that of the models trained with original fe atures. In particular, the accuracy with AE-compressed feature s reached the highest, even overwhelming the original features in some cases. We strongly believe that our approach lessens the insufficient training corpus problem by reducing the redun dancy in the high-dimensional features. For the classifier mod el, the MLP almost always outperforms other models in classif ying the signal in the compressed/original feature setup. Hence, we suggest utilizing MLP based on AE-compressed features f or efficient signal classification.

### **Chapter 2. Related Work**

One of the most prominent problems in paralinguistic sign al processing studies is speech emotion recognition, as it is a crucial factor in optimal human-computer interaction, including dialog systems [8]. The challenge that speech emotion recogn ition poses is predicting the emotion behind the speech and cla ssifying it into one of the following categories: happy, sad, neu tral, and angry. To achieve this goal, classic machine learning a lgorithms, such as the hidden Markov model (HMM), support v ector machines (SVM), and decision trees, have been adopted [9]-[11]. Later, several studies started utilizing deep learning architectures for speech emotion recognition. A feedforward neural network has been used to extract window-level feature s, summarize them into a single utterance-level feature with s ome statistical functions, and generate an output prediction wit h an extreme learning machine (ELM) [12]. Since the deep ne ural network with ELM model estimates the probability for eac h frame of small window length, Lee et al. [13] suggested a d eep bidirectional long short-term memory (LSTM) architecture on a low-level acoustic feature set to incorporate long contex tual effect and to avoid the vanishing gradient problem. As an effort to consider regionally salient information within a signal, Aldeneh et al. [14] extracted 40-dimensional log Mel filterba nk features (MFBs) from the raw signal and applied convolutio n layers, max-pooling layers, and dense layers followed by a softmax layer to categorize each utterance into emotion label s.

# **Chapter 3. Task Description**

This paper concentrates on two paralinguistic tasks that inv olve classification problems using a small amount of data (i.e., 5 02, 3342 training instances) with high-dimensional features. Ou r objective in each task is to build a model that achieves the b est classification accuracy. To evaluate the performance of the model, we use weight accuracy recall (WAR), the ratio of corre ct predictions to the whole test samples, which is widely used in this study.

The heartbeat classification task: This task focuses on distinguis hing anomalies of heartbeat sounds. The given types of heartbea t sounds are "normal", "mild", and "moderate" and "seve re" (heart disease). For this task, the Heart Sounds Shenzhen (HSS) corpus is gathered from 170 subjects (115 male/55 fem ale, ages ranging from 21 to 88). The data set includes 502, 1 80 and 163 utterances for training, validation, and testing, respe ctively.

The atypical affect classification task: An emotion of disabled sp eakers is recognized. The emotion classes are defined as "ang ry", "happy", "sad" and "neutral". To gather the Emotion al Sensitivity Assistance System for People with Disabilities (E motAsS) dataset, 15 mentally, neurologically, or physically disa bled individuals (7 male / 8 female, ages ranging from 20 to 5 8) were recorded spontaneously in a familiar room in their wor kplace. Under the supervision of a psychologist, five different ta sks were performed to generate emotional utterances: describin g images, talking about specific topics, telling a story of a pictu red book, introducing their everyday business, and playing toget her games. The corpus contains 3342 and 4186 utterances for training and testing, respectively [15], [16].

### **Chapter 4. Proposed Framework**

#### 4.1. Feature sets

To explore feature reduction effects on various feature sett ings, we use the Interspeech 2018 ComParE [17] and emobase features extracted using the openSMILE toolkit [18] on all task corpora. These features include signal processed features such as mel-frequency cepstral coefficients (MFCC), F0, and log me l frequency. In addition, they contain statistical functional featur es within certain time frames. The dimensions of the features within each utterance is fixed to 6,373 and 1,582 in ComParE and emobase, respectively.

#### 4.2. Compression methods

In this study, various machine learning techniques are sugg ested for feature dimension reduction to investigate its efficac y on two different feature sets. These techniques include not only classical approaches such as PCA and LDA but also recen t neural network-based AEs.

**Principal component analysis (PCA):** PCA is an unsupervised le arning technique that aims to identify the principal components that maximize the variance of transformed data points. Compres sed test features are obtained by transforming original test features with pretrained PCA parameters. We use PCA for compr essing features into 2- and 200-dimensional spaces (PCA-2 and PCA-200, respectively).

Linear discriminant analysis (LDA): Unlike PCA, the LDA uses the label information of the training set so that it minimizes th e distance between the same labels and separates data points belonging to different labels as much as possible. To perform t his, we find a linear transformation that maximizes the ratio of "between class scatter" and "within class scatter". Unlike PCA and AE, we set the dimension of the latent code vector a s N-1, where N is the number of classes in the training corp us.

Autoencoder (AE): This is basically a neural network encoding the original feature vector into a latent vector of small dimens ions and decoding the latent vector into the reconstruction vecto r of the original dimension. We use the mean square error (MS E) between the original feature vector and the reconstruction vector as a loss function, which aims to efficiently contain info rmation on the original features in the latent vector. For the im plementation, we use three dense layers with a Selu activation function [19] and batch normalization to stabilize the training procedure. To avoid overfitting, we adopt early stop criteria w hen the validation MSE loss starts to increase. With the traine d model, we extract latent vectors by encoding the original fea tures of the training and testing dataset. In all tasks, ComParE and emobase features of the training set are encoded into 400 – and 200–dimensional Euclidean space, respectively.

#### 4.3. Classification methods

Four classical classifiers and neural network-based model are used for our tasks.

**Logistic regression (LR):** As a basic classification model, it use s a logistic function with trainable parameters to assign a prob ability for each label given each feature. The parameters are u pdated through gradient descent. Support vector machine (SVM): The goal of the support vector machine is to find a decision boundary that maximizes the classi fication margin between the data points in different classes given all the label information. Based on these pre-trained parameter s for the decision boundary, new instances are predicted to belong to the label of the highest probability. We implemented linear SVM in our experiments.

**Decision tree (DT):** A decision tree comprises three types of n odes: the root node, internal nodes, and terminal nodes. The ro ot node and the internal nodes contain features that determine the path of the training example. The construction of the tree s tructure starts with the root node, and the iterative dichotomise r 3 (ID3) algorithm selects the feature of each node. The algorit hm chooses the attribute with the maximum information gain wi thin each iteration.

**Gradient Boosting tree (XGB):** The boosting tree is essentially a weighted ensemble of weaker decision trees that optimizes a multiclass objective function [20]. We achieve this by recurrent ly adding a new decision tree function at every round. To mak e the model properly learn the structures of trees and the data, the loss function in each iteration is defined as the error betwe en the model's prediction at each round and true value. The re gularization term of each additive tree is added to alleviate ove rfitting on the training set and to promote a better generalizatio n of the whole model.

Multilayer perceptron (MLP): Multilayer perceptron is part of an artificial neural network, which comprises input nodes, hidden nodes, and output nodes. In our experiments, two hidden layers followed by a softmax layer with the Selu activation function

[19] were used for nonlinear transformation. We also applied b atch normalization and dropout with probability 0.2. All backpro pagated parameters were updated to minimize the loss function at each epoch.

## **Chapter 5. Performance Evaluation**

TABLE I

MODEL PERFORMANCE COMPARISONS FOR THE HEARTBEAT TASK. The TOP-2 PERFORMANCES ARE MARKED IN BOLD.

Feature	Compression	LR	SVM	DT	XGB	MLP
ComParE	-	50.92	42.33	41.10	53.99	55.83
	AE	50.92	54.60	41.72	53.37	55.83
	PCA-2	30.06	37.68	33.74	49.08	54.60
	PCA-200	38.65	49.08	38.65	53.37	53.99
	LDA	49.69	50.31	52.15	52.76	51.53
Emobase	-	50.92	53.37	39.26	57.06	55.83
	AE	57.67	37.42	38.65	57.67	57.06
	PCA-2	55.83	55.21	40.49	49.08	55.21
	PCA-200	44.79	57.06	45.40	53.37	57.67
	LDA	42.94	44.17	41.72	41.10	44.79

TABLE II MODEL PERFORMANCE COMPARISONS FOR THE ATYPICAL TASK. The TOP-2 PERFORMANCES ARE MARKED IN BOLD.

Feature	Compression	LR	SVM	DT	XGB	MLP
ComParE	-	67.13	43.38	51.12	66.67	67.80
	AE	67.82	59.99	50.38	66.15	67.87
	PCA-2	33.85	22.62	49.93	66.20	67.56
	PCA-200	38.13	45.99	49.57	67.30	67.80
	LDA	42.33	45.48	45.39	38.70	39.94
Emobase	-	64.14	66.60	51.82	66.29	66.67
	AE	64.19	64.02	49.73	66.32	64.43
	PCA-2	68.01	36.19	49.07	67.49	67.96
	PCA-200	65.50	36.62	52.20	67.56	65.86
	LDA	55.02	55.02	48.78	50.00	54.95

#### 5.1. Heartbeat classification task

Table I demonstrates the results of the heartbeat classificatio n task. Overall, the best performance (57.67%) was obtained u sing MLP with PCA-200 compressed emobase features and LR /XGB with AE-compressed emobase features. In general, the M LP classifier outperformed the other four classification models i n both the original/compressed feature setups. Additionally, DT is worse than XGB in most cases, as it is a simplified version of XGB. For the experiments with MLP, we stopped training when the validation loss started increasing to avoid overfitting.

# 5.2. Atypical affect classification task

As shown in Table II, using LR and MLP with PCA-2 emob ase features achieved 68.01% and 67.96%, respectively. Howev er, when considering all five training models, we observed that the AE-compressed features result in the highest average acc uracy. Furthermore, the MLP classifier performed better than other models in most feature/compression settings. For the im plementation, we divided the training corpus into an 8:2 ratio f or the training/validation set.

# **Chapter 6. Discussion**



Fig. 1. Visualization of PCA compression.



Fig. 2. Visualization of AE compression.

#### 6.1. Compression ability of AE

In two tasks, it was clearly observed that the combination of AE compression and the MLP classifier had very competitive p erformance in all tasks, even better than that of using the orig inal emobase feature set. This shows the efficacy of the appro ach to training small amounts of data and high dimensions. To i nterpret these phenomena, we first compressed the ComParE f eatures of the heartbeat training set into the 200-dimensional Euclidean space by PCA and selected 2 dominant principal com ponents of each data for visualization, which were plotted in Fi g. 1. With these trained parameters of PCA, we compressed the ComParE features in a testing set into 2-dimensional space. For visualization of AE compression, we selected two components of the first and second largest absolute values among each 400-dimension train/test compressed vector because their acti

vations are the most influential for the classification process.

As shown in Fig. 2, the AE-compressed data points belongin g to the same classes in the train/test set are comparatively w ell clustered together, whereas data in different classes are se parated. Furthermore, they are aligned linearly with an almost identical gradient, which makes the distribution of the test set features close to the training set's feature distribution. Howeve r, the distinction of PCA-compressed data points in different c lasses is apparently harder than the AE compression case. We consider all these factors to make AE better than the PCA co mpression method.

#### 6.2. Classification with MLP

As described above, our experimental results reveal that MLP almost always outperforms other classifiers both in original an d compressed feature settings, overcoming data insufficiency. T his demonstrates that neural network architecture can still learn b etter representations with the compressed feature. In addition, we expect to see continual improvements with neural architectu re variants in future works in general paralinguistic signal classi fication tasks.

# **Chapter 7. Conclusion**

In this paper, we propose the implementation of compression frameworks for paralinguistic signal classification tasks. We extr act two sets of features (ComParE, emobase2010) for training our models and explore how they vary in the aspect of classific ation accuracy among the heartbeat and atypical affect classifica tion tasks. We train our models with our original features and t he features autonomously compressed by PCA, LDA, and AE.

From the experiments, we observe that AE compression feat ures and the MLP classifier are two key factors for achieving s uperior classification accuracy. Furthermore, they show even be tter performances than that of the combination with non-compr essed features, which contain more information on the signal. T hese results demonstrate that the AE-compressed features can practically alternate original features that suffer from high dime nsions when the size of the training corpus is limited.

Finally, we show by comparison that the MLP generally achie ves a better ability to learn feature representations than classic al models in two paralinguistic tasks.

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준언어적 신호를 분류를 인식하고 분류하는 일은 그의 다양한 응용성 측면에서 매우 중요한 문제이다. 일반적으로 이 문제가 어려운 이유는 소리 정보가 인간에게도 구별되기 힘들다는 애매모호한 특성 때문이다. 이에 신호를 더 잘 이해하기 위해 기계학습 기법이 고안되는데, 이 때 분석에 사용되는 신호 특징 벡터는 운율, 에너지, 주파수 등 신호에 관 련된 정보로 이루어진 고차원 벡터이다. 즉 훈련에 사용되는 데이터의 크기가 작은 경우에는, 특징 벡터의 높은 차원 때문에 적절히 기계학습 모델을 잘 훈련시키기가 어렵게 된다. 이 논문에서는 심층 신경망 모델 을 이용하여 이와 같은 문제를 해결하고자 한다. 우선 다양한 압축 기법 을 이용하여 특징 벡터 내의 불필요한 정보를 제거하고, 이 압축된 특징 들이 전통적 기계학습 분류방법들보다 심층 신경망에 의해 더 잘 분류됨 을 실험적으로 보인다.

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