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10:50	(초청논문)고감도 표면 플라즈몬 공명 광학 바이오칩의 제작 및 응용 .....	55
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11:20	(초청논문)파장재활용방식의 WDM/TDM Hybrid PON 시스템 BMT 및 상용 서비스 .....	67
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11:50	문턱전류 부근에서 동작시킨 DFB를 주입하여 반사 민감도를 개선시킨 RSOA 기반 WDM-PON ..	69
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# Detection of Avian Influenza-DNA Hybridization using a Wavelength Interrogation-based Surface Plasmon Resonance Biosensor

파장측정용 표면플라즈몬공명 센서를 이용한 조류독감 DNA 의 혼성화 검출

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## Abstract

A wavelength interrogation-based surface plasmon resonance (SPR) biosensor has been investigated for a detection of avian influenza DNA (AI-DNA). The immobilization of oligonucleotides and hybridization reaction of AI-DNA was monitored in real time without labeling. The results showed that SPR biosensor can provide linear detection suitable for quantification of AI-DNA. This study demonstrates the potential for a simple AI virus diagnosis. Since these viruses can be transmitted into humans and often are fatal, improved AI detection is important.

Since avian influenza viruses (AIVs) not only lead to economic losses but also cause a fatal disease in humans, a rapid screening of AIVs is required [1]. Various virological detection methods, involving virus isolation and RT-PCR, have been introduced for AIVs detection. However, they require relatively long measurement time, complex experimental sequences, and expensive huge facilities. To overcome these limitations, it is desirable to develop a rapid, label-free, and highly specific detection method to identify an AIV infection.

Surface plasmon resonance (SPR) is well-known as an effective technique without any labeling [2]. This method is also applicable *in situ* real time monitoring, because the plasmon waves can detect the DNA hybridization kinetics immediately. In this study, we employed a wavelength interrogation SPR method for

a quantitative detection of AI-DNA hybridization.

## 1. SPR setup and materials

We used three different oligonucleotides, as listed in Table 1. Target probe was originated from A avian influenza (NY/73-63-6/00(H7N2)) hemagglutinin.

A gold film with a thickness of 45 nm was sputtered on a SF10 slide glass with a 5nm chromium adhesion layer. We used a custom-made Kretschmann-configuration optical setup to detect SPR signals as shown in Fig. 1. An incidence angle was fixed at 60° for wavelength scanning from 550 to 650 nm. Two PDMS microfluidic (working and reference) channels were placed on the SPR sensor chip and all SPR measurements were carried with a flow rate of 2  $\mu$ l/min. The resonance wavelength was determined by fitting the reflectance curve to the second-order

polynomial equation. In addition, the reflectance characteristics of s-polarized light had been recorded to eliminate various noise components depending on the wavelength of light source.

Name	Sequence (5'-3')	Description
Capture probe (C <sub>1</sub> )	Thiol- <u>TTT TTT TTT TTT TTT</u> ATT GGA CAC GAG ACG CAA TG	35-mer oligonucleotide with 15-mer Thymine (underlined) as a spacer.
Target probe (T <sub>1</sub> )	CAT TGC GTC TCG TGT CCA AT	Complementary oligonucleotide
Mismatched target probe (T <sub>2</sub> )	CAT TGC GTC TGC <u>ACA</u> GGT TA	Ten-base (underlined) mismatched oligonucleotide

Table 1. The sequence of used oligonucleotides

## 2. Results

To estimate the detection efficiency of our SPR system, the sensitivity was assessed by measuring the dependence of SPR signal on ethanol concentration. The minimum value of measurable refractive index variation was determined to be about  $1.6 \times 10^{-4}$  in refractive index unit (RIU).

Next, the hybridization process was performed by injecting of 1  $\mu$ M T<sub>1</sub> and T<sub>2</sub> probes without additional labeling, respectively. An obvious reaction was observed on the working channel where a solution of T<sub>1</sub> was injected, while no significant change was found for a solution of T<sub>2</sub> (Fig.2 inset). The result confirms the specificity of the assay procedure.

For wavelength interrogation SPR to be useful quantitatively, it is important that changes of resonance wavelength can be linearly proportional to changes of the concentration, and thus to the amount of bound analytes. Figure 2 shows the experimental

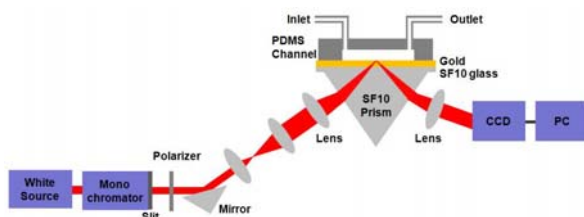


Fig.1. Schematic diagram of SPR measurement system

result when T<sub>1</sub> was diluted in the hybridization buffer. The values of resonance wavelength were equal to  $0.59 \pm 0.16$  nm,  $1.75 \pm 0.25$  nm,  $2.77 \pm 0.34$  nm, and  $4.84 \pm 0.24$  nm to the T<sub>1</sub> concentrations of 1, 2, 3, and 5  $\mu$ M, respectively. Using the linear function of  $y = ax$ , we found that the proportional constant ( $a$ ) equals 0.9377 with  $R^2 = 0.9835$ . The results indicate that the wavelength interrogation SPR sensor has a highly linear dynamic range to be useful quantitative detection.

## 3. Conclusion

We have confirmed that a wavelength-scanning type SPR biosensor can provide a label-free, real-time, and specific detection of AI-DNA hybridization with a highly linear performance. This indicates that the wavelength interrogation SPR system is suitable for an application of AI-DNA hybridization detection for a simple AI virus diagnosis.

[1] J. Xu et al., "Detection of avian influenza virus using an interferometric biosensor", Anal. Bioanal. Chem. Vol. 389, pp. 1193-1199, 2007.

[2] A. J. Thiel, et al., "In situ surface plasmon resonance imaging detection of DNA hybridization to oligonucleotide arrays on gold surfaces," Anal. Chem. Vol. 69, pp. 4948-4956, 1997.

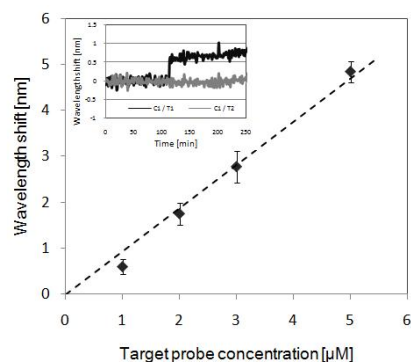


Fig.2. SPR wavelength shift at different target DNA concentrations